



Hard X-ray phase contrast microscopy and fluorescence mapping with KB optics

P. Cloetens^a

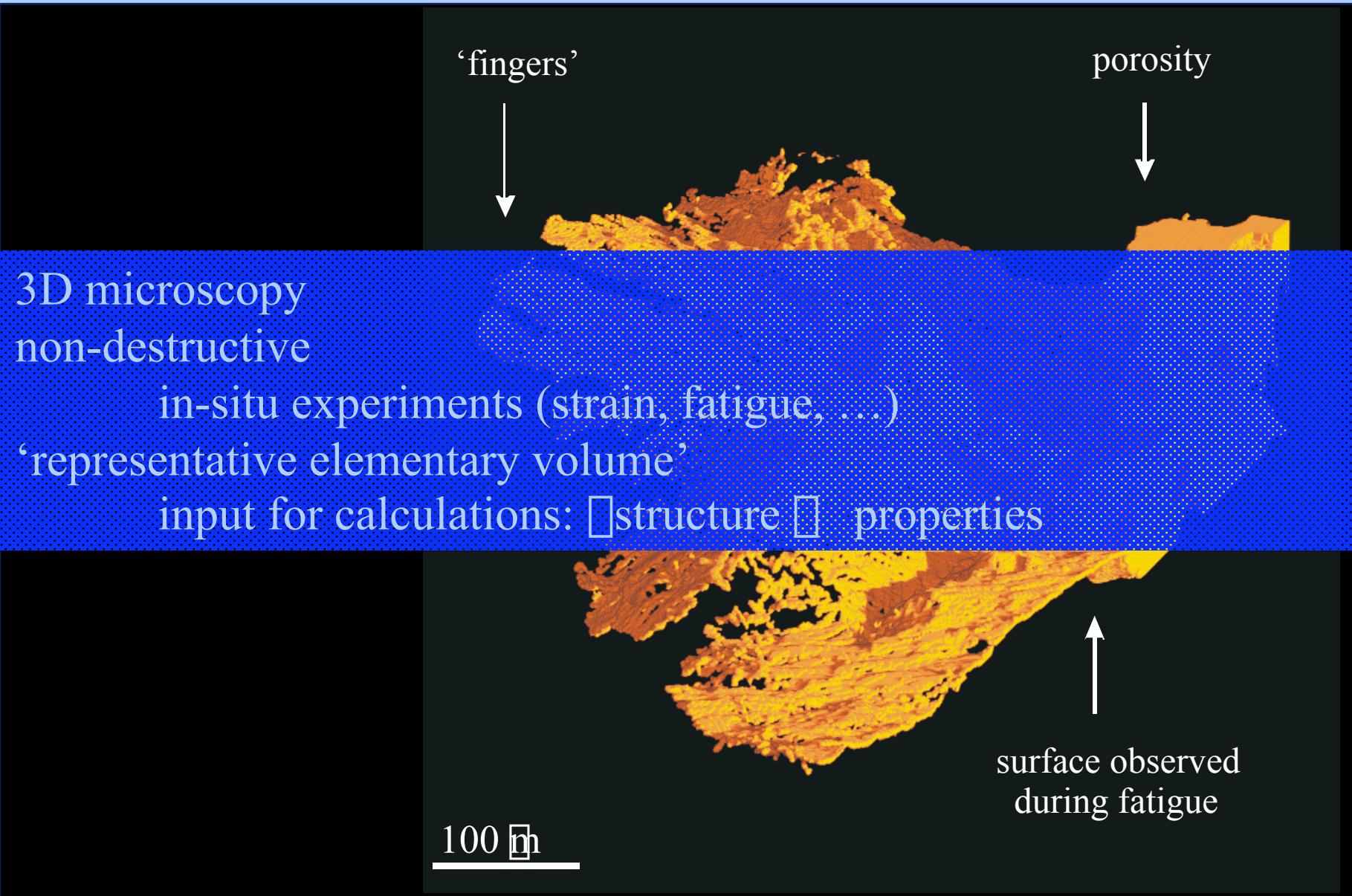
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W. Ludwig^b, S. Bohic^a, E. Pereiro^a

a ESRF, Grenoble

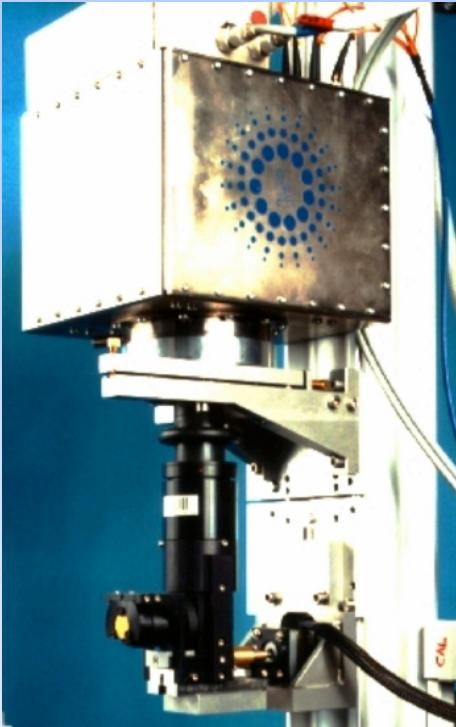
b GEMPPM, INSA Lyon, France

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Motivation



Motivation



Improve the spatial resolution

resolution $\leq 0.5 \mu\text{m}$

NA=0.95, 1 μm thick LAG:Eu, 11.5 keV
with scintillator based detectors

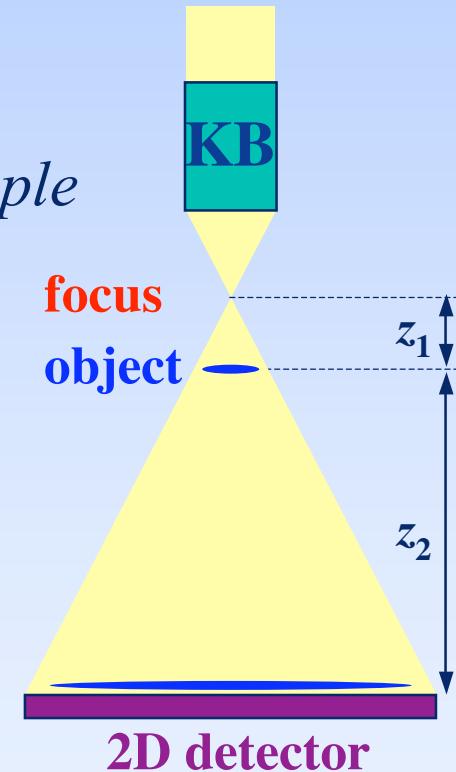
X-ray magnification using

diffractive optics (FZP)
refractive optics (CRL)
reflective optics (KB)

Motivation

Gabor's Microscopic principle (Nature, 1948)

The object is illuminated by an electron beam brought to a fine focus... The object is a small distance behind (or in front) of the point focus, followed by a photographic plate at a large multiple of this distance...



Outline

KB optics

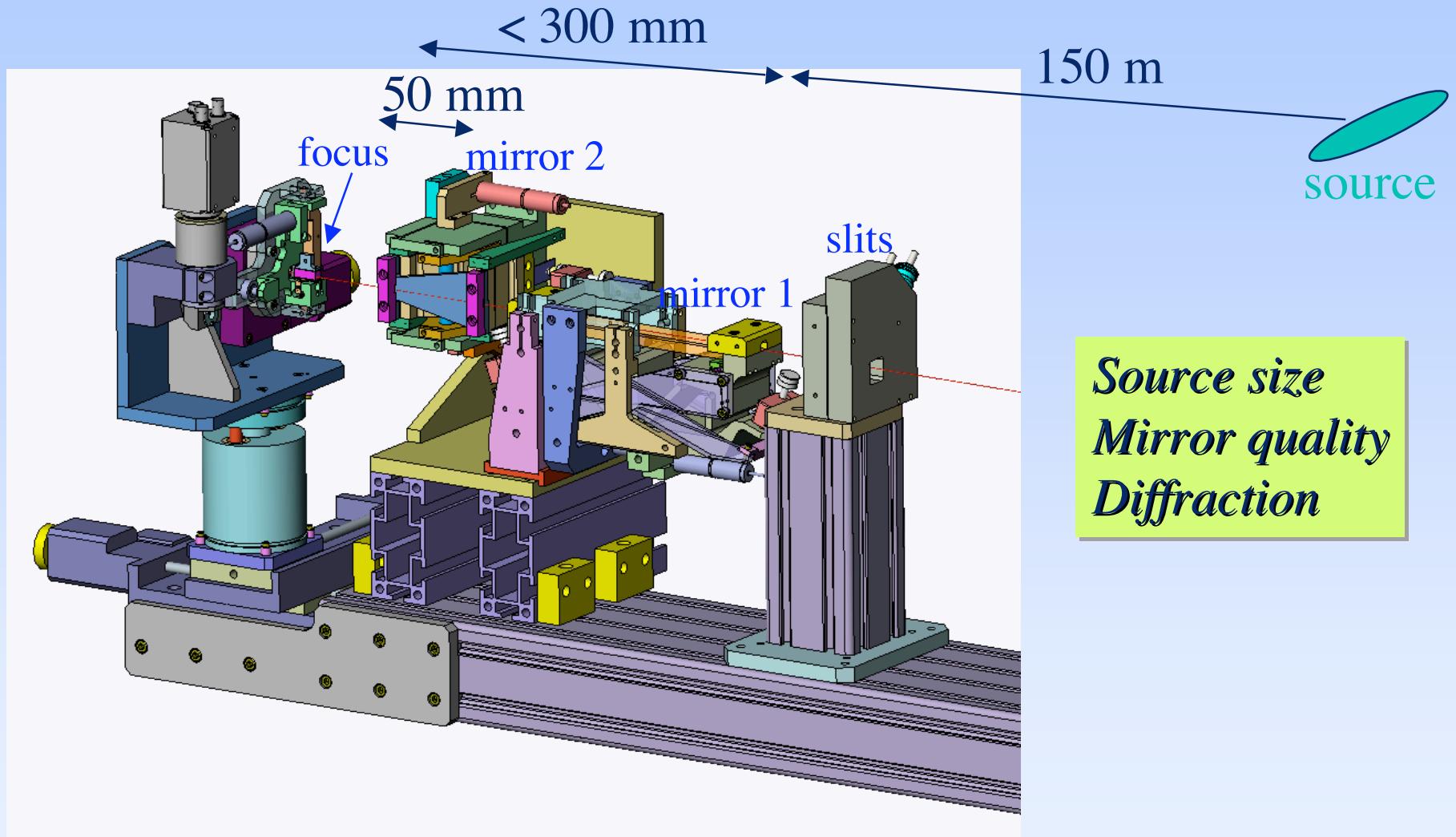
- Limits in KB focusing
- Measurement of the spot size

Applications

- Projection Microscopy
- Fluorescence imaging

Prospects

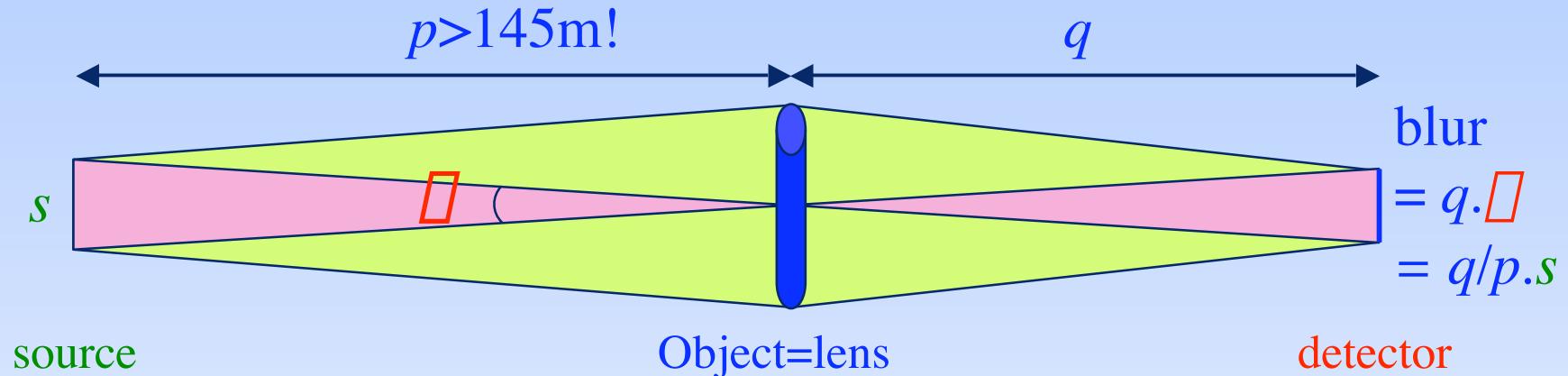
Kirkpatrick-Baez focusing



Limits in KB focusing

Source size

Focus = Demagnified image of the source



Same requirement as for Phase Contrast Imaging

Source ID19


125 nm(h) * 25 nm (v)
Low section!

Demagnification = p/q

Hor.: 1540
Ver.: 520

focus


87 nm * 45 nm

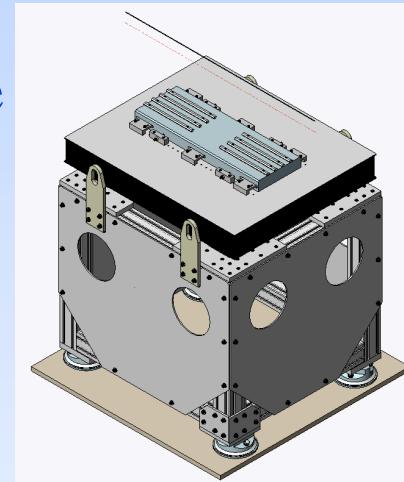
Limits in KB focusing

‘Effective’ Source size

Vibrations!

should be smaller than angular source size (0.15 rad fwhm)

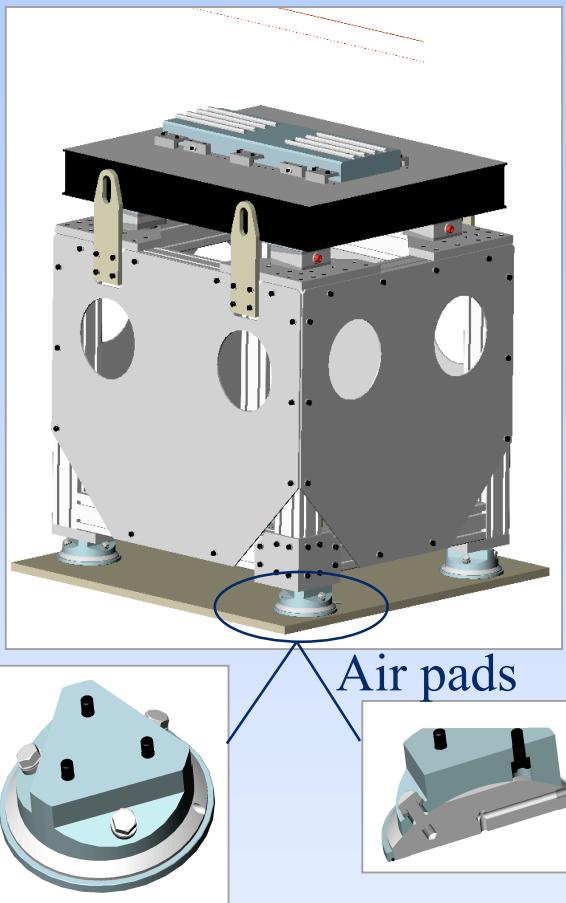
- *Complete instrument on a single table light and rigid structure*



KB-table
P. Bernard

- *No pre-monochromator* (cooling)
Multilayer on first mirror as monochromator
Enormous gain in *flux*
Gain in *vertical acceptance*
□ $E/E \approx 10^{-2}$ (3d harmonic undulator)

Light frame KB table

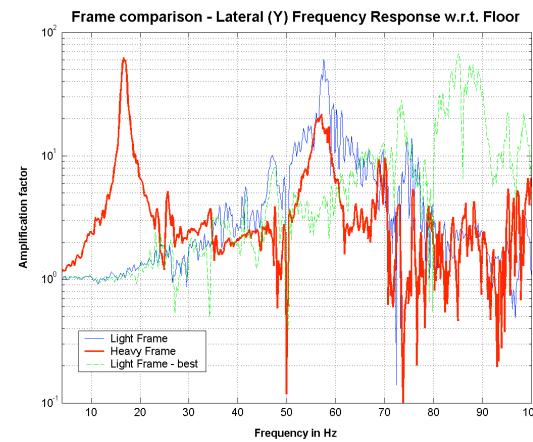


Natural frequency above floor excitation

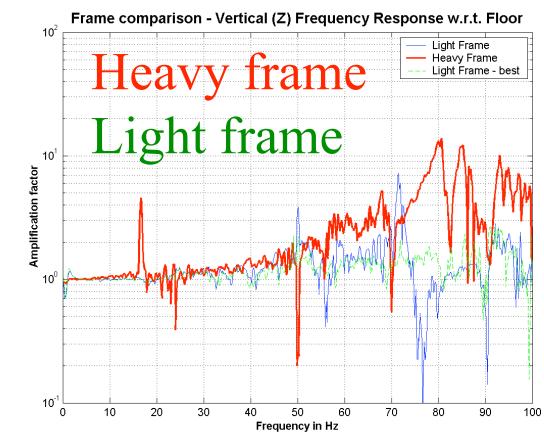
$$f_{\text{res}} = \frac{1}{2\pi} \sqrt{\frac{k}{m}}$$

High stiffness
Light

Lateral amplification



Vertical amplification

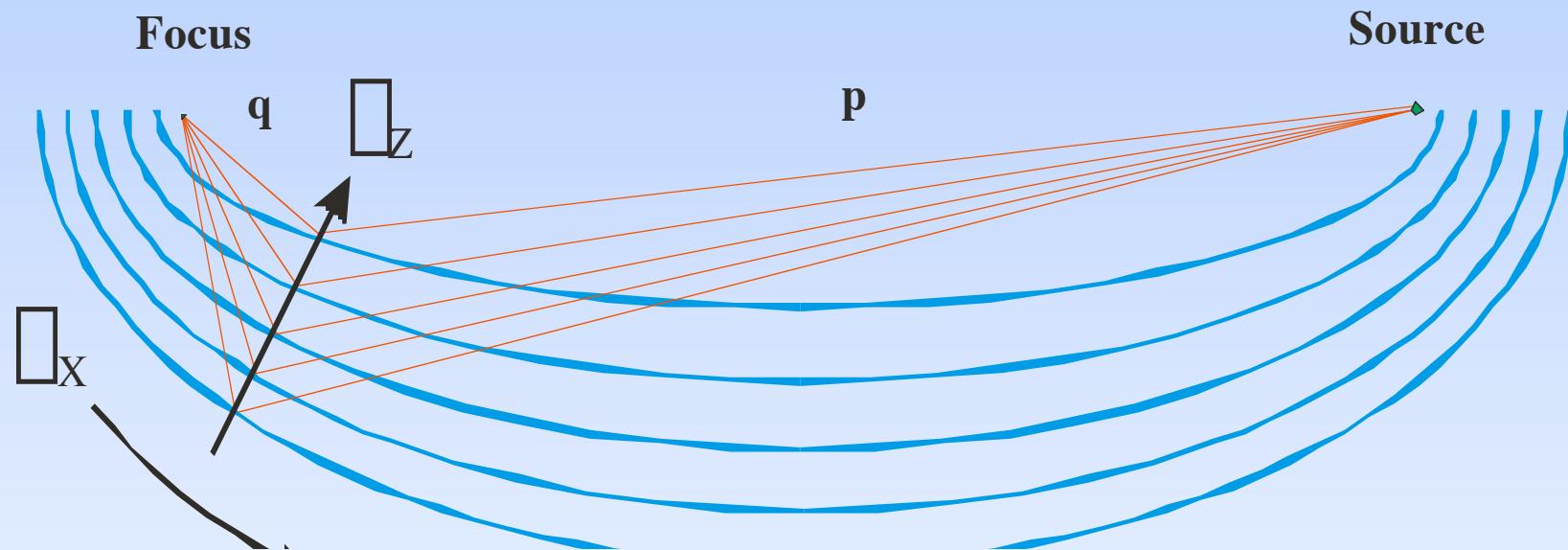


		Vertical (Z) [m]			Longitudinal (X)			Lateral (Y)			Δy Rotation [rad]
		Floor	Top plate	Rel. %	Floor	Top plate	Rel. %	Floor	Top plate	Rel. %	
Heavy Frame	dpp	0.76	0.83	9.7	0.94	1.2	27.8	0.46	1.97	326.7	0.25
	rms	0.12	0.13	5.5	0.09	0.12	44	0.07	0.29	291	0.04
Light Frame	dpp	0.67	0.69	2.5	0.31	0.33	7.7	0.49	0.53	7.6	0.09
	rms	0.11	0.11	1.5	0.05	0.05	3.1	0.07	0.07	4.9	0.01

Δy
10 nrad
rms

Multilayer coating

Incidence angle variation up to 50% → laterally graded multilayer
Depth gradient negligible ($< 10^{-5}$)

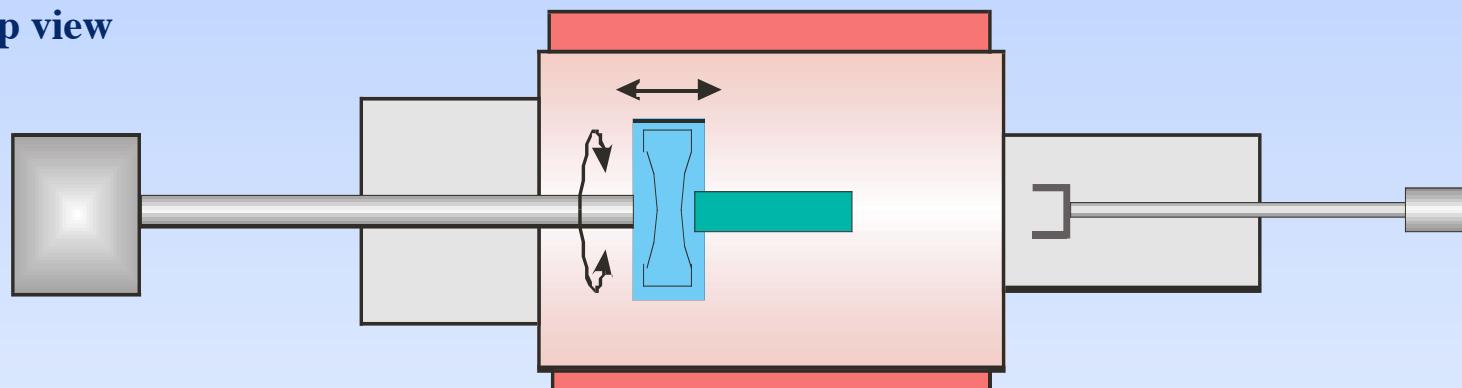


Multilayer coating

ESRF deposition facility

- Distributed Electron Cyclotron Resonance (DECR) plasma sputtering
- 3 target positions, rotation and linear movement

Top view



Base pressure

10^{-8} mbar

Ar pressure

1.3×10^{-3} mbar

Polarization voltage

$U = -500 \dots -2000$ V (DC/RF)

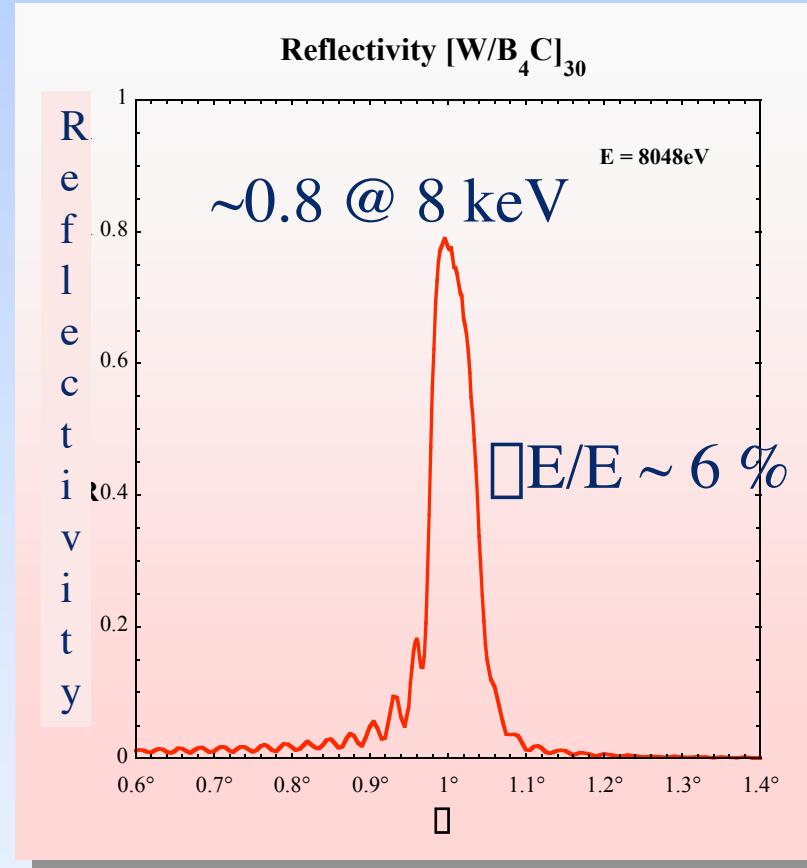
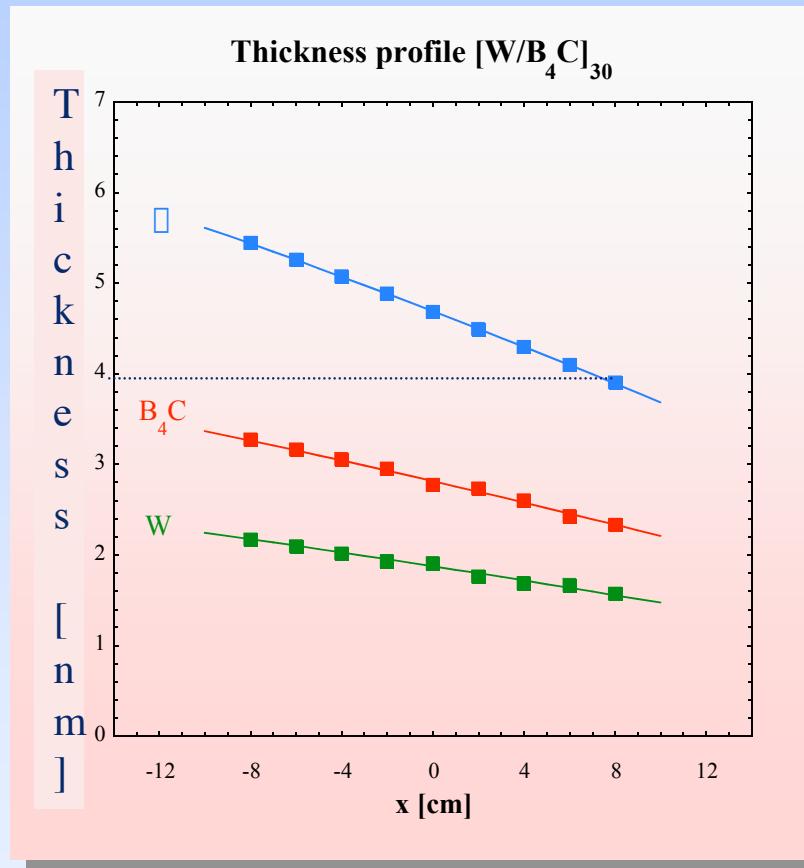
Particle flux

$R = 0.02 \dots 0.10$ nm/s

Deposition temperature

$T_{Depo} \leq 100^\circ\text{C}$

Multilayer coating



Limits in KB focusing

Mirror quality

Elliptical shape

Incoherent view point

Slope errors \square

$$\text{Blur} = 2. \square . q$$

Coherent view point

$$\text{Shape errors } h \square \text{ Aberrations}$$
$$\square \square = -4 \square / \square . h . \sin \square$$

Use small region of mirror

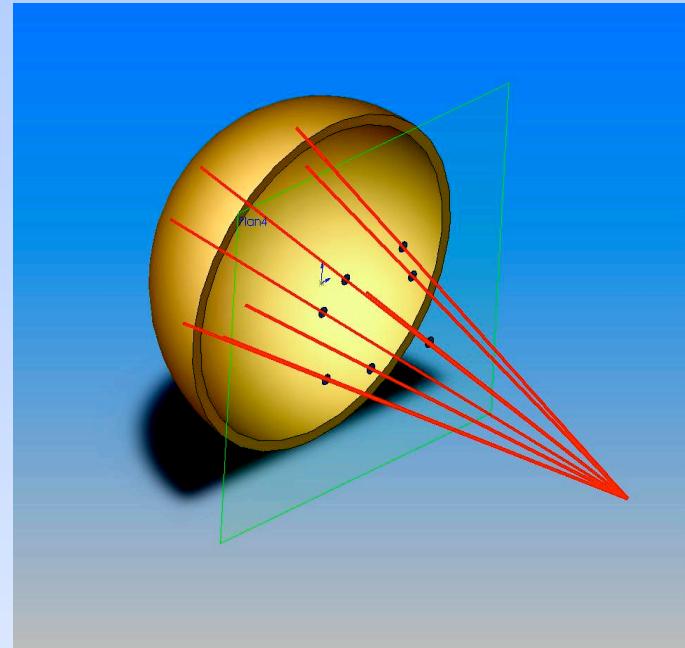
Mirrors manufactured by Wave Precision

Dynamical bending

2 actuators / mirror

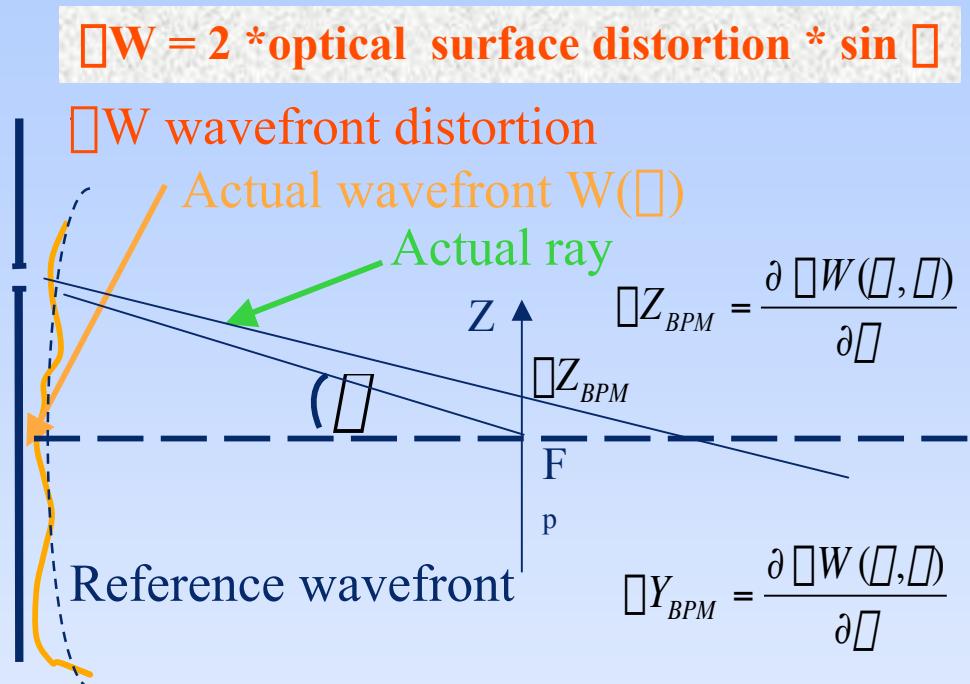
automatic alignment procedure

Alignment procedure



Wavefront W = equiphase surface
Normal rays defined by slits

BeamPositionMonitor = XCCD



Measuring $\square Z_{BPM}$ with scanning slit and BPM
Integrating \rightarrow Optical surfaces information

Alignment procedure

Linear optimization

interaction matrix scheme

- Measure the linear information \mathbf{Y} (slope)
- Send a unit displacement on each actuator
- Store the resulting system differential metrology ∂Y
- Build the interaction matrix \mathbf{H} by grouping all ∂Y
- Correction vector \mathbf{C} to be sent to the actuators

$$C = (H^T H)^{-1} H^T Y$$

Limits in KB focusing

Diffraction

Numerical aperture should be sufficiently large

$$\text{‘Blur’} = c \frac{\square}{w} q \quad w = \text{slit width}$$

Use large region of the mirror

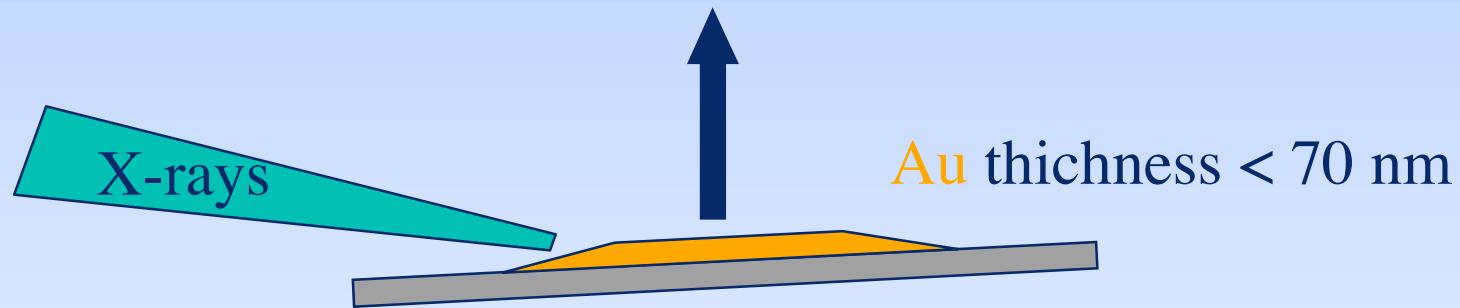
Focusing results at 20.5 keV

Measurement:

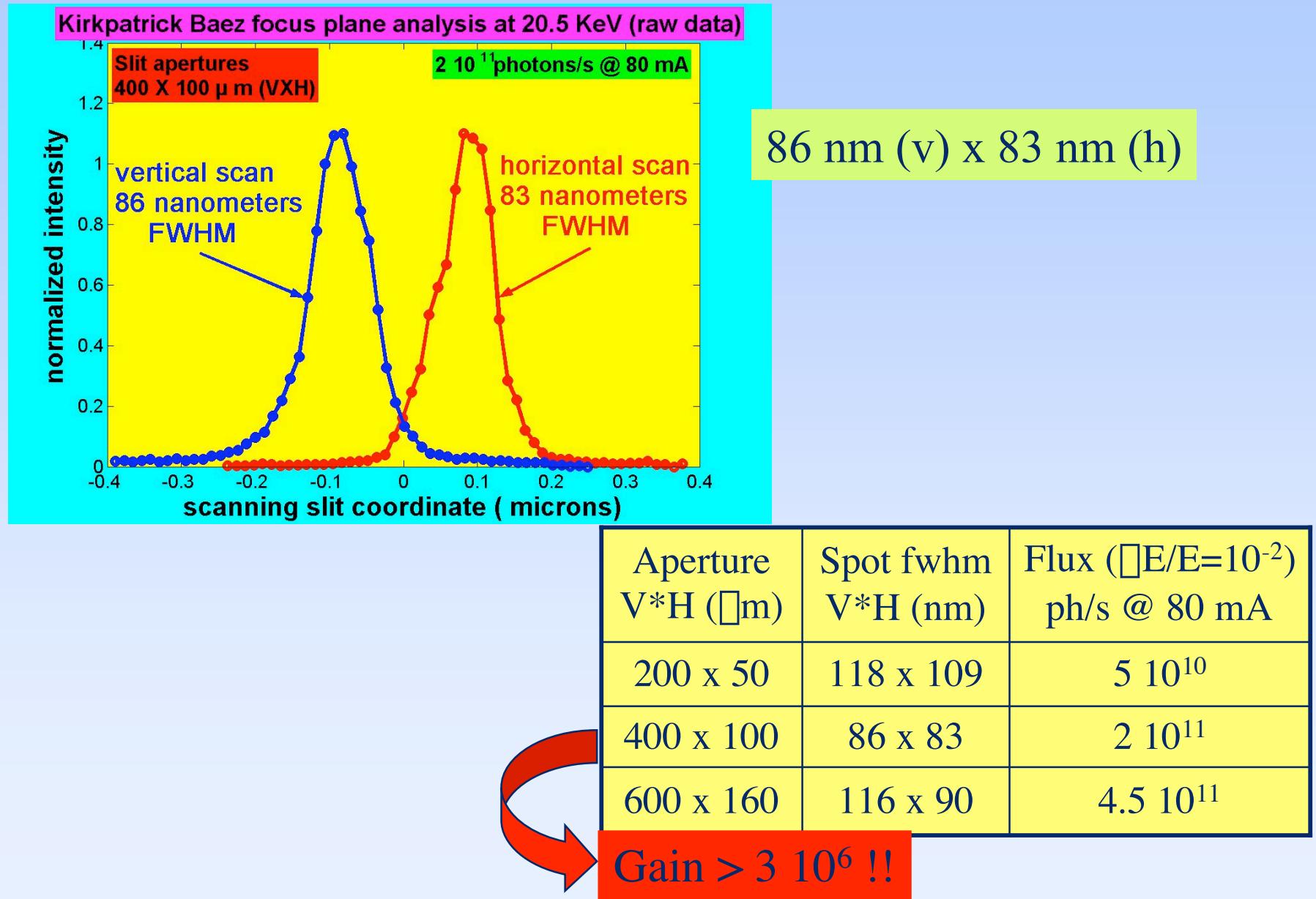
Direct line scan, no derivation

Fluorescence of Au slit

More direct and precise than an edge scan



Focusing results at 20.5 keV

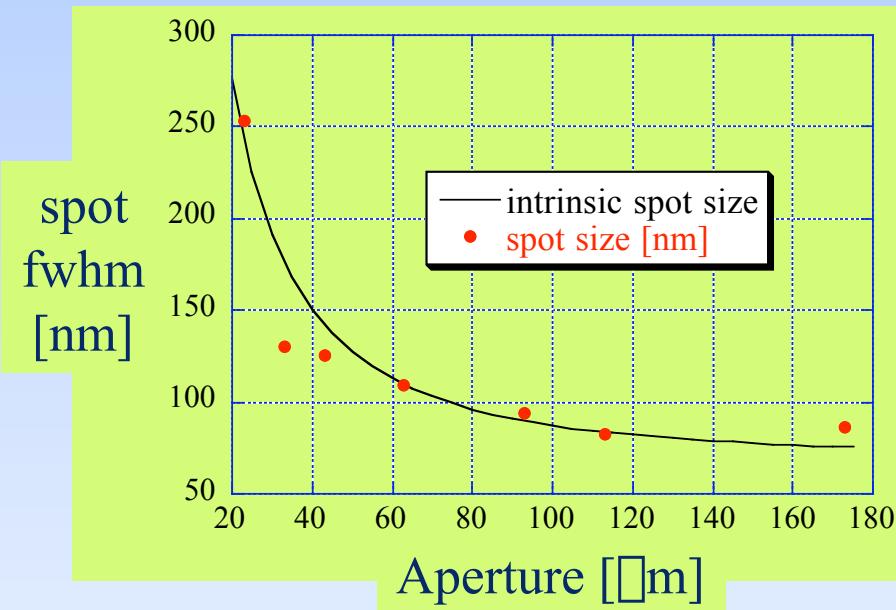


O. Hignette, P. Cloetens

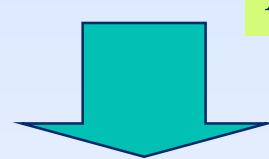
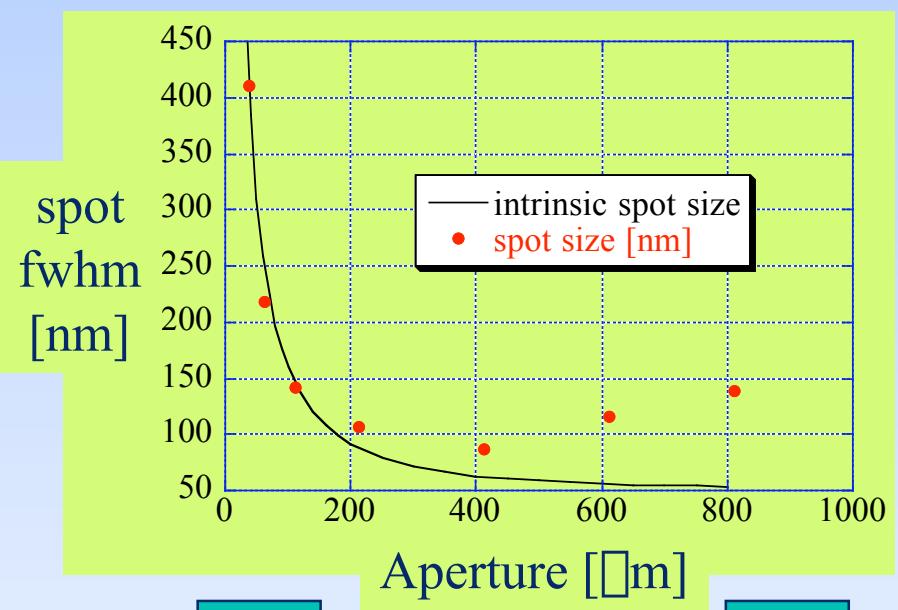
Focusing results at 20.5 keV

Effect of the aperture

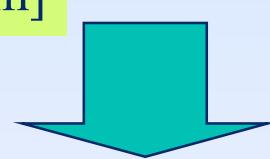
horizontal



vertical

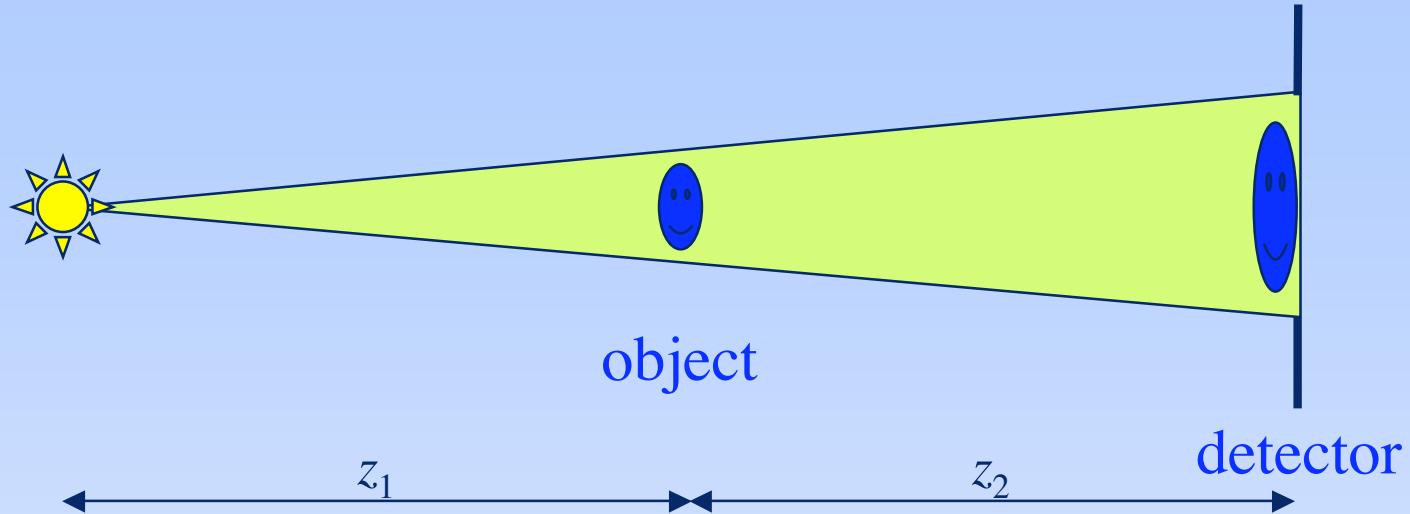


Diffraction limited

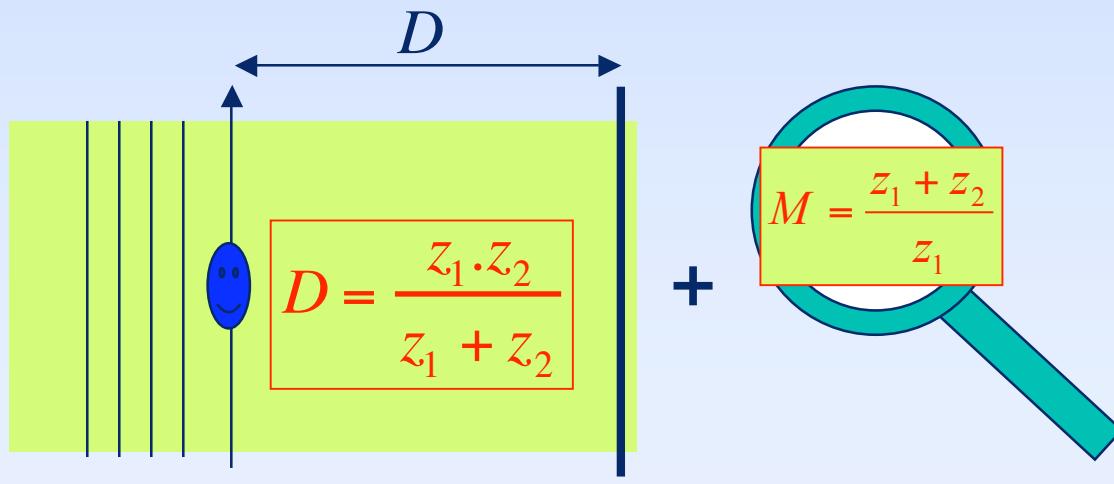


Increase tails

Applications: Projection Microscopy



equivalent to



Limit cases

$$z_1 \gg z_2$$

$$D = z_2 ; M = 1$$

$$z_1 \ll z_2$$

$$D = z_1 ; M = z_2/z_1$$

Projection Microscopy

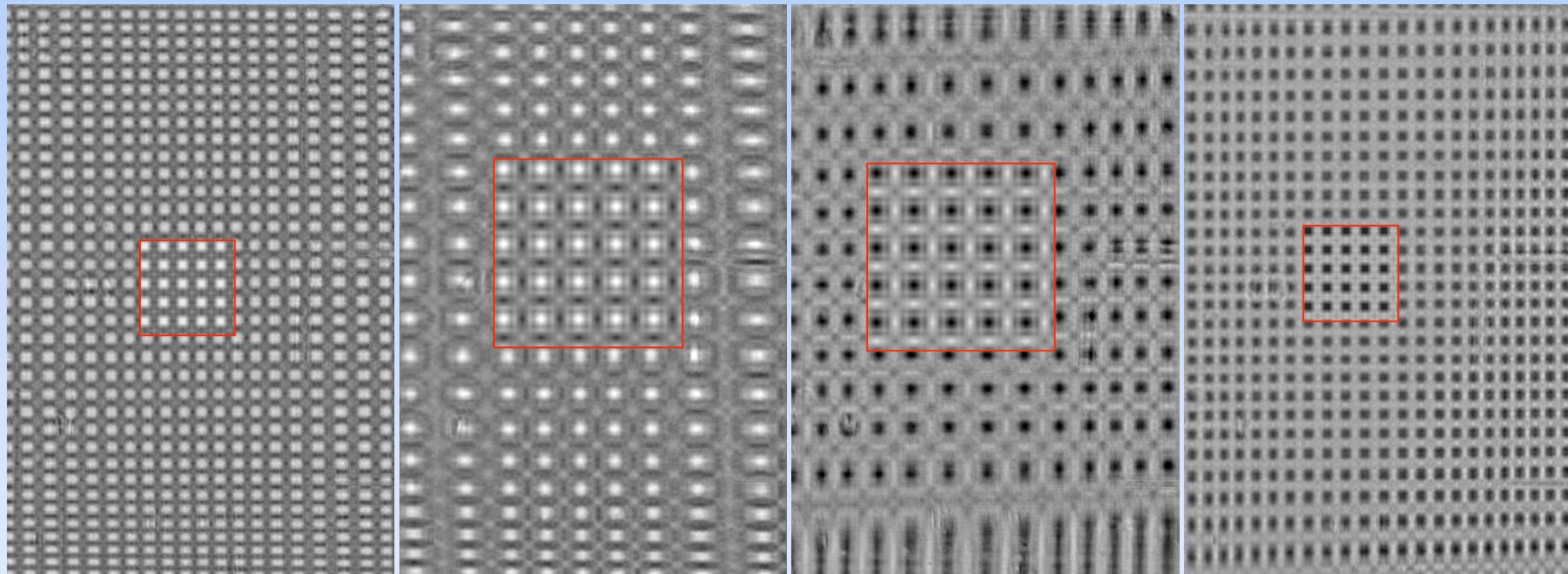
2 \AA m pitch grating (Si)

C. David, PSI

10 \AA m

Mirrors fully illuminated

0.2 (H) x 1.1 (V) mm, $E=20.5$ keV



$D = -20 \text{ mm}$

$M = 115$

$D = -10 \text{ mm}$

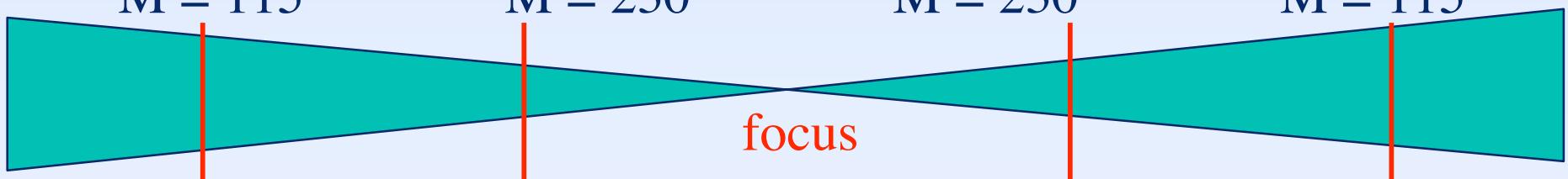
$M = 230$

$D = 10 \text{ mm}$

$M = 230$

$D = 20 \text{ mm}$

$M = 115$

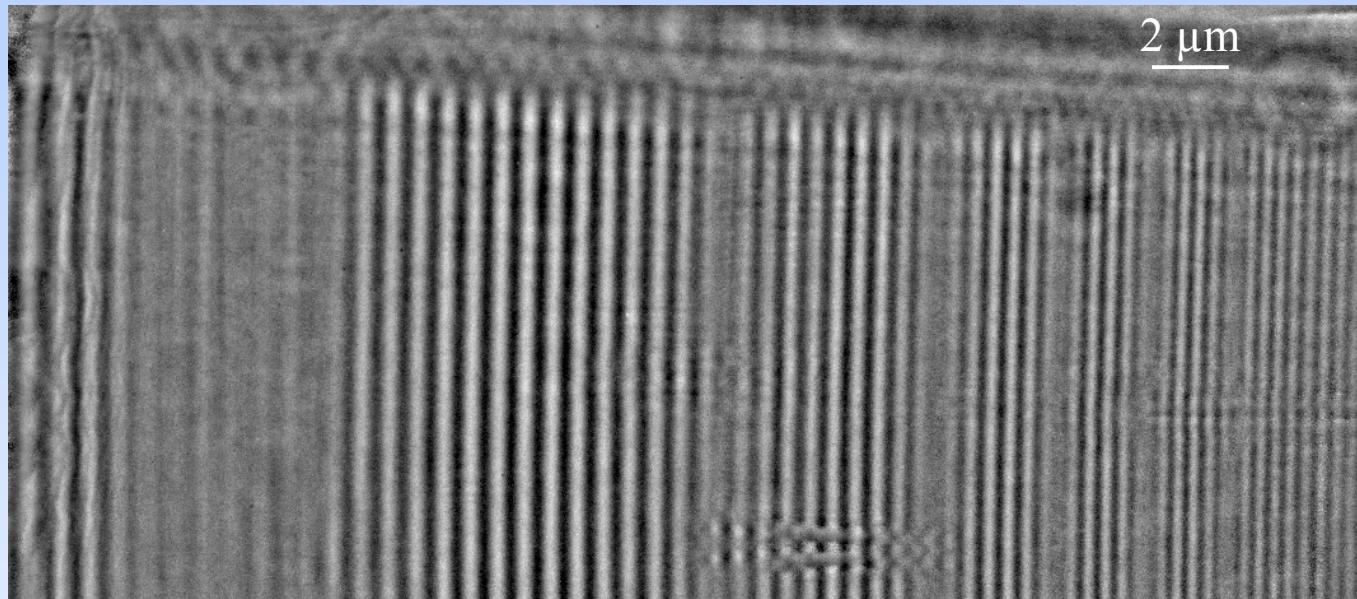


Exposure time = 0.4 s ! (16-bunch, saturation CCD)

P. Cloetens, O. Hignette

Coherent imaging

Decreasing linewidth
Increasing spatial frequency



Object invisible !

period ≈ 720 nm

period ≈ 610 nm

period ≈ 530 nm

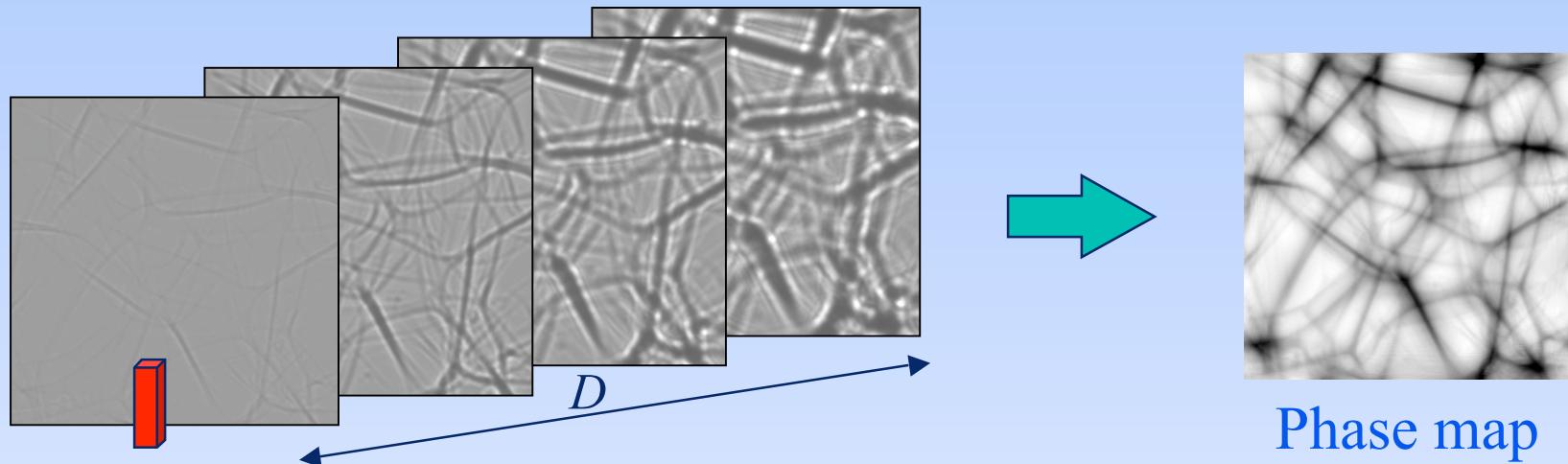
Sample by M. Panitz,
University of Goettingen

Contrast depends strongly on period or spatial frequency

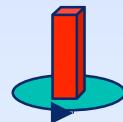
Phase retrieval

Poster 6.106

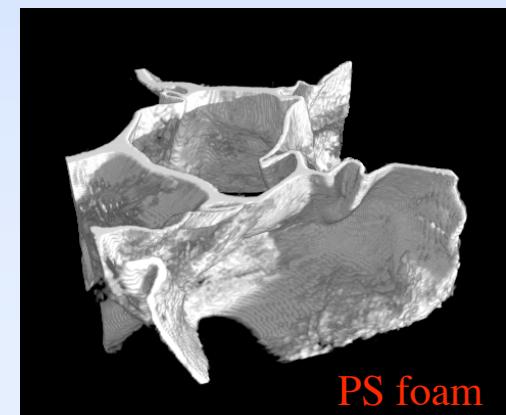
1) phase retrieval with images at different distances



2) tomography: repeated for \square 1000 angular positions

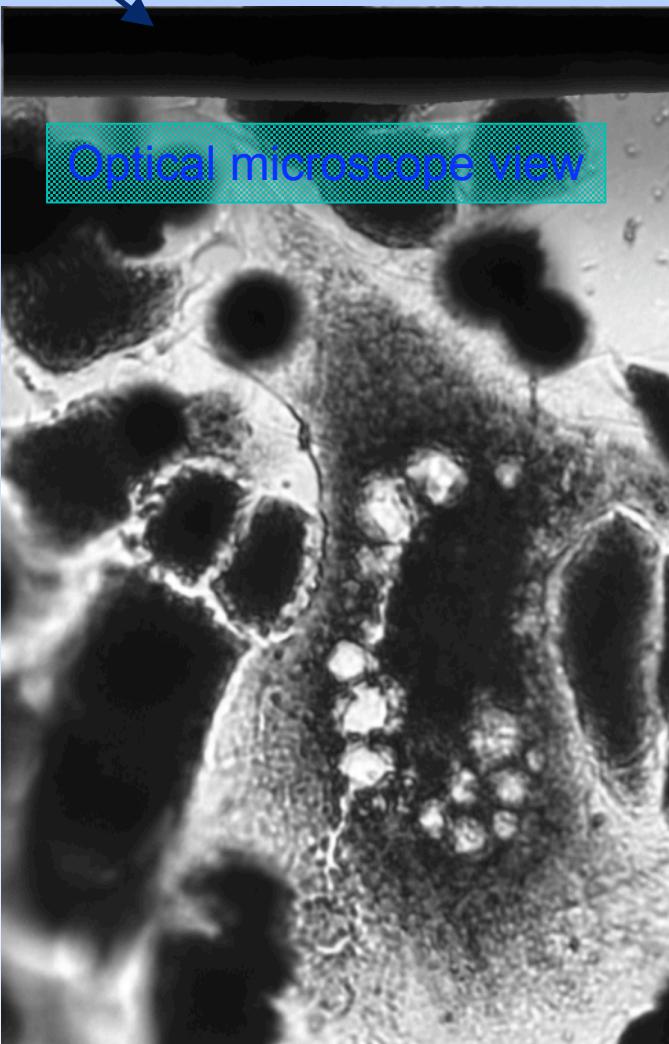


3D distribution of \square or the electron-density
improved resolution
straightforward interpretation
processing

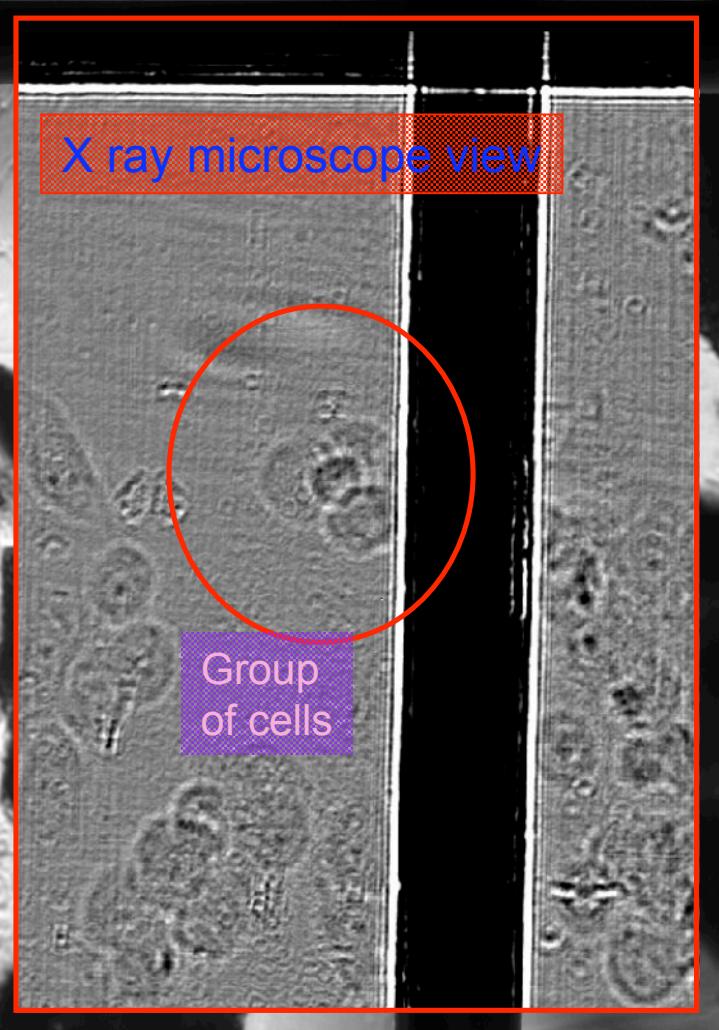


Projection Microscopy

Cu fiber



Optical microscope view



X ray microscope view

Group
of cells

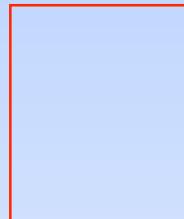
25 μm

Cellular imaging Cancerous cells
S. Bohic

Projection Microscopy

Cancerous cells
S. Bohic

Towards focus



10 μ m

$D = 50 \text{ mm}$
 $M = 45$

$D = 30 \text{ mm}$
 $M = 75$

$E = 20.5 \text{ keV}$

Exposure time = 0.3 s ! (16-bunch)

$D = 10 \text{ mm}$
 $M = 230$

No X-ray optics behind the sample \square dose efficient

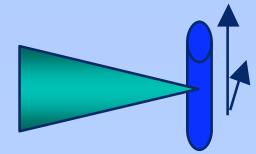
P. Cloetens, W. Ludwig

Applications: Fluorescence

Cancerous cells treated with anti-cancer drug (Cisplatin)

Step = 0.3 μm , 0.9 sec/pt

40 μm



K

Pt

$E = 15 \text{ keV}$

Phase Contrast

Fe

P. Cloetens,
W. Ludwig,
S. Bohic

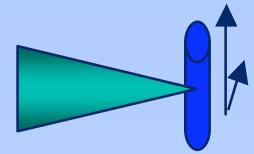
Applications: Fluorescence

Cancerous cells (Coll. S. Bohic- ID22)

50 μm

K

Pt



Step = 0.5 μm
1 sec/pt

Fe

Traces of Pt-based drug can be imaged
New opens in elemental cellular chemistry

Adapted length scale for

- sub-cellular structures (cell organelles)
- unicellular organisms (bacteria, algae and fungi)

Prospects

Nano-tomography

Starting in October

Next generation synchrotrons

Present source size limit with KB:

90 nm x 50 nm

(Source size)

(Mirror quality: ion beam figuring)

Diffraction

ultimate focus: 20 nm (h) x 12 nm (v)

Much more efficient:

0.2 mm x 1.2 mm of a 20 mm x 3 mm beam



Conclusions

- Sub $(90 \text{ nm})^2$ focusing made ‘easy’ for hard X-rays
- High flux ($5 \cdot 10^{11} \text{ ph/s}$ @ 200 mA)
thanks to KB efficiency, multilayer optics
- Micro-structure: fast nano-radiography, nano-tomography
 - + : fast and dose efficient full-field imaging
good resolution (sub 100 nm in both directions)
 - : distortions due to mirror quality
 - +/- : defocused image = phase contrast image
- Fluorescence: probe for sub-micron element mapping (2D - 3D)



Acknowledgments

KB Optics

- Optics Group ESRF
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- Beamline contact
 - P. Bernard
- SciSoft ESRF
 - E. Chinchio
- Bliss ESRF
 - D. Fernandez

Experiments

- S. Zabler, K. Fezzaa (APS), W.K. Lee (APS)

Samples

- Ch. David PSI
- M. Panitz University of Goettingen